

ARTICLE

Open Access

Ultrasensitive liquid sensor based on an embedded microchannel bulk acoustic wave resonator

Xiyu Gu¹, Yan Liu²✉, Yuanhang Qu³, Xiang Chen³, Zesheng Liu³, Yao Cai³, Wenjuan Liu³, Shishang Guo^{1,4}✉ and Chengliang Sun^{3,4}✉

Abstract

The high-frequency and high-quality factor characteristics of bulk acoustic wave (BAW) resonators have significantly advanced their application in sensing technologies. In this work, a fluidic sensor based on a BAW resonator structure is fabricated and investigated. Embedded microchannels are formed beneath the active area of the BAW device without the need for external processes. As liquid flows through the microchannel, pressure is exerted on the upper wall (piezoelectric film) of the microchannel, which causes a shift in the resonant frequency. Using density functional theory, we revealed the intrinsic mechanism by which piezoelectric film deformation influences BAW resonator performance. Theoretically, the upwardly convex piezoelectric film caused by liquid flow can increase the resonant frequency. The experimental results obtained with ethanol solutions of different concentrations reveal that the sensor, which operates at a high resonant frequency of 2.225 GHz, achieves a remarkable sensitivity of 5.1 MHz/% (221 ppm/%), with an ultrahigh linearity of 0.995. This study reveals the intrinsic mechanism of liquid sensing based on BAW resonators, highlights the potential of AlN/Al_{0.8}Sc_{0.2}N composite film BAW resonators in liquid sensing applications and offers insights for future research and development in this field.

Introduction

Owing to their excellent stability, resolution, and accuracy, as well as their low cost, compact size, and properties that allow devices to be easily interfaced with digital systems, resonators have attracted widespread interest in the detection and characterization of liquids. The ability to detect the concentration of liquids in a mixture is critical for many applications, such as water quality assessment¹, chemical processing², environmental monitoring³, and bio-sensing⁴. Resonator-based fluidic sensors monitor liquids through changes in the spectral response of the resonator, such as the quality factor (Q), resonance amplitude, and resonant frequency. Resonators commonly used as sensors can be divided into microwave resonators and piezoelectric resonators. Some studies have investigated split ring

resonators (SRRs) and their derived resonator structures to realize high-sensitivity fluid sensors based on microwave resonators^{5,6}. However, miniaturization, integration, anti-interference, and high sensitivity remain major challenges for fluid sensors in the detection and characterization of binary mixtures. The size of microwave resonators is larger than that of piezoelectric resonators. An increasing number of studies have investigated piezoelectric resonators to achieve compact size and high-sensitivity sensors based on piezoelectric resonators^{7,8}.

Piezoelectric resonators are known for their precise control of frequency⁹. Bulk acoustic wave (BAW) resonators, as tiny piezoelectric devices manufactured by microelectromechanical systems (MEMS), have significant advantages as high-precision resonant sensors¹⁰, including smaller size, complementary metal oxide semiconductor (CMOS) compatibility, higher sensitivity, and low fabrication and measurement costs¹¹. In addition, BAW resonators, as sensors that convert physical signals to electrical signals, have the advantage of high frequency, which can avoid interference. With the maturity of the BAW resonator manufacturing process, an increasing

Correspondence: Yan Liu (liuyan92@whu.edu.cn) or Shishang Guo (gssyhx@whu.edu.cn) or Chengliang Sun (sunc@whu.edu.cn)

¹Key Laboratory of Artificial Micro, and Nano-structures of Ministry of Education, School of Physics and Technology, Wuhan University, Wuhan 430072, PR China

²School of Mathematical and Physical Sciences, Wuhan Textile University, Wuhan 430200, PR China

Full list of author information is available at the end of the article

number of types of sensors based on BAW resonators have been designed. Using a BAW resonator, Yan et al. fabricated a mass sensor with a high sensitivity of 8–10 kHz cm²/ng at 3–4 GHz¹². He et al. investigated the pressure sensing of a BAW resonator with a sensitivity of approximately –17.4 ppm kPa^{–1,13}.

BAW resonators also show great application potential in liquid sensors. Link et al. utilized a BAW resonator to detect water and 59% glycerol¹⁴. Vorobiev et al.¹⁵ and Rezazadeh et al.¹⁶ demonstrated the potential of the BAW resonator in characterizing the viscosity of liquids. Chen et al. fabricated a BAW resonator with c-axis tilted AlN films to achieve a sensitivity of 15 Hz cm²/μg for liquid loading¹⁷. In 2017, Liang et al. designed a glucose sensor with a sensitivity of 10.8 MHz/M through a glucose solution flowing on a BAW resonator¹⁸. Zhou et al. extended the application of BAW resonators in liquid viscosity sensing¹⁹. However, the intrinsic mechanism of resonant liquid sensors based on BAW resonators is lacking.

In this work, we presented a high-sensitivity liquid sensor with an embedded microchannel under the AlN/

AlScN BAW resonator, with the same fabrication process (6 masks) as the BAW resonator, as shown in Fig. 1a. Through the application of DFT calculations and finite element methods (FEMs), it was discovered that the frequency drift of the BAW resonator is caused by the deformation of the piezoelectric film, which is influenced by the liquid flow beneath the resonator, as shown in Fig. 1b, c. Different frequency drifts can reflect the concentration and type of liquid. These experimental results are in good agreement with our simulation results.

Theory and design

Based on the frequency sensitivity of the BAW resonator, we designed embedded microchannels under BAW resonators for ultrasensitive sensing in liquids, as shown in Fig. 1a. This high-sensitivity liquid sensor has a low fabrication cost because it uses the same fabrication process (6 masks) as the BAW resonator. In this design, when liquid flows through the microchannel under the action of droplet pressure, the piezoelectric film under the microchannel will undergo mechanical deformation, as shown in Fig. 1b. The pressure formula of liquid flow on the microchannel wall is given by

$$P = \frac{8\mu\nu l}{d_h^2} \quad (1)$$

where μ is the fluid viscosity, ν is the average fluid velocity, l is the unit flow length, and d_h is the hydraulic diameter of the microchannel. According to Formula (1), the deformation of the microchannel wall is directly influenced by the fluid viscosity.

The deformation of the piezoelectric film under the microchannel was investigated via the FEM when different liquids flow through the microchannel, as demonstrated in Fig. 2. As water with different velocities flows through the microchannel under the BAW resonator, the piezoelectric film deforms more as the flow speed increases, as depicted in Fig. 2a–c. Table 1 lists the peak

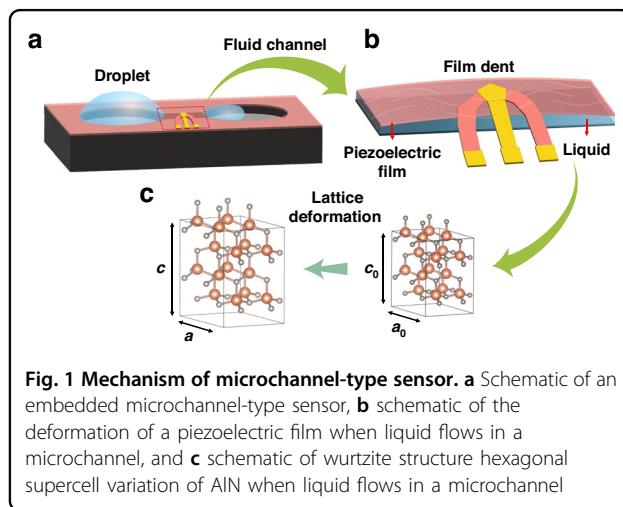


Fig. 1 Mechanism of microchannel-type sensor. **a** Schematic of an embedded microchannel-type sensor, **b** schematic of the deformation of a piezoelectric film when liquid flows in a microchannel, and **c** schematic of wurtzite structure hexagonal supercell variation of AlN when liquid flows in a microchannel

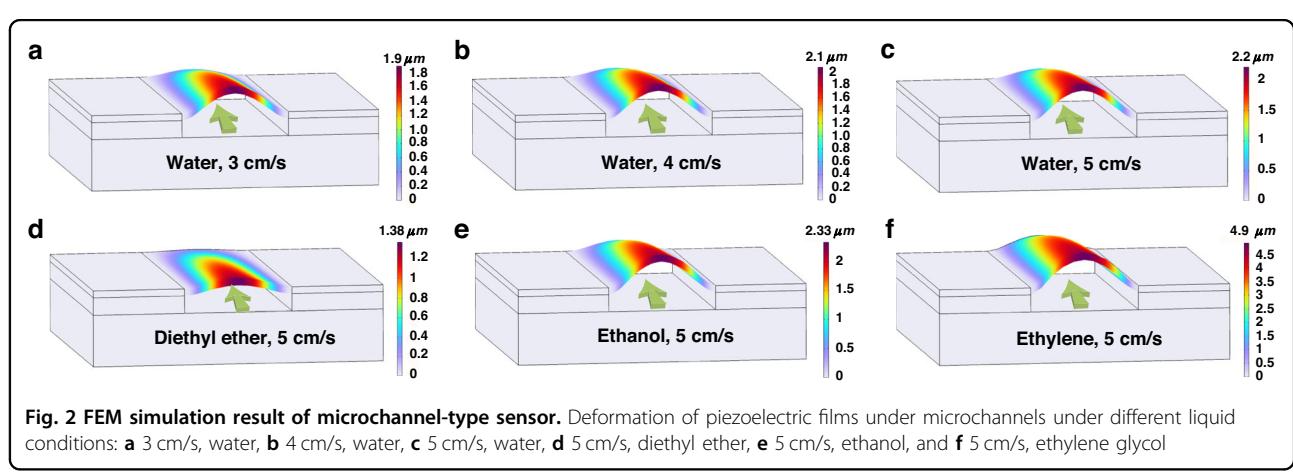


Fig. 2 FEM simulation result of microchannel-type sensor. Deformation of piezoelectric films under microchannels under different liquid conditions: **a** 3 cm/s, water, **b** 4 cm/s, water, **c** 5 cm/s, water, **d** 5 cm/s, diethyl ether, **e** 5 cm/s, ethanol, and **f** 5 cm/s, ethylene glycol

displacement values of piezoelectric films under microchannels with various water velocities. When liquids with the same velocity are different, the deformations of the piezoelectric film are different. We select a variety of liquids (water, diethyl ether, ethanol, and ethylene glycol) to simulate the deformation of piezoelectric films under microchannels. Table 2 lists the viscosity parameters of these liquids at 25 °C. As shown in Fig. 2c–f, the deformation of the piezoelectric film increased as the viscosity of the liquid increased. Table 2 lists the peak displacement values of piezoelectric films under microchannels with various liquids flowing at 5 cm/s. These simulation results are consistent with the theoretical formula calculations. These different types of film deformation caused by different liquid flows directly affect the performance of the BAW resonator. These findings show that the embedded microchannels under BAW resonators have great application potential in ultrasensitive sensing in liquids.

As the liquid flows through the microchannels under the resonator, the film bulges because the main effect of the z-direction is pressure on the film. This film deformation directly changes the lattice structure of the film material, which changes its physical properties. The mechanical and piezoelectric properties of piezoelectric materials are intrinsically linked to the resonant frequency and the effective electromechanical coupling coefficient of BAW resonators^{20,21}. These characteristics significantly increase the potential of BAW resonators for sensing applications.

To analyze the effect of piezoelectric film bulging (the main effect of the z-direction exerting pressure) on the performance of the resonator, the change in the AlN lattice at different pressures in the z-direction is calculated. Through the first-principles software Material Studio (MS), which is based on density functional perturbation theory (DFT)²², a 32-atom hexagonal supercell of wurtzite AlN was constructed and used in calculations, as shown in Fig. 1c. The generalized gradient

approximation of Perdew–Burke–Ernzerhof (GGA–PBE) was utilized to calculate the exchange-correlation total energy²³. The first Brillouin-zone integrals are performed on a Monkhorst–Pack mesh of $9 \times 9 \times 3$ k-points, and the plane wave cutoff is set to 570 eV. For precise calculation, the crystalline structures of $2 \times 2 \times 2$ AlN used for calculation are a-axis lattice constants (a) and c-axis lattice constants (c), as depicted in Fig. 1c.

The pressure directly affects the a -axis and c -axis lattice constants of the film material²⁴. To calculate the change in the AlN lattice at different pressures in the z direction, the linear response method was utilized with the Cambridge Sequential Total Energy Package (CASTEP)^{22,23,25}. As presented in Fig. 3a, the a and c lattice constants had opposite linear relationships with the z-direction pressure in the range of -2 GPa to 2 GPa. The a lattice constant has a negative linear relationship with the z-direction pressure, and the c lattice constant has a positive linear relationship with the z-direction pressure. This law is consistent with the deformation of some materials under z-direction pressure²⁶.

Moreover, as depicted in Fig. 3b, the lattice volume (V) also has a positive linear relationship with the z-direction pressure, and the lattice density (ρ) has a negative linear relationship with the z-direction pressure. These lattice changes directly affect physical properties, such as piezoelectric properties and the elastic stiffness tensor.

To obtain the elastic constants under different pressures in the z-direction, crystalline structures deformed at different pressures were computed via CASTEP. The variation in the relative elastic constants with pressure (x) can also be found in the calculation results, as shown in Fig. 3c. In the range of -2 GPa to 2 GPa, this trend was fitted by quadratic Eqs. (2)–(6):

$$c_{11}(x) = 0.2388x^2 - 2.4968x + 367.542 \quad (2)$$

$$c_{12}(x) = 0.2744x^2 - 1.8903x + 123.237 \quad (3)$$

$$c_{13}(x) = 0.1425x^2 - 4.6558x + 92.858 \quad (4)$$

$$c_{33}(x) = -0.9146x^2 + 12.9104x + 339.25 \quad (5)$$

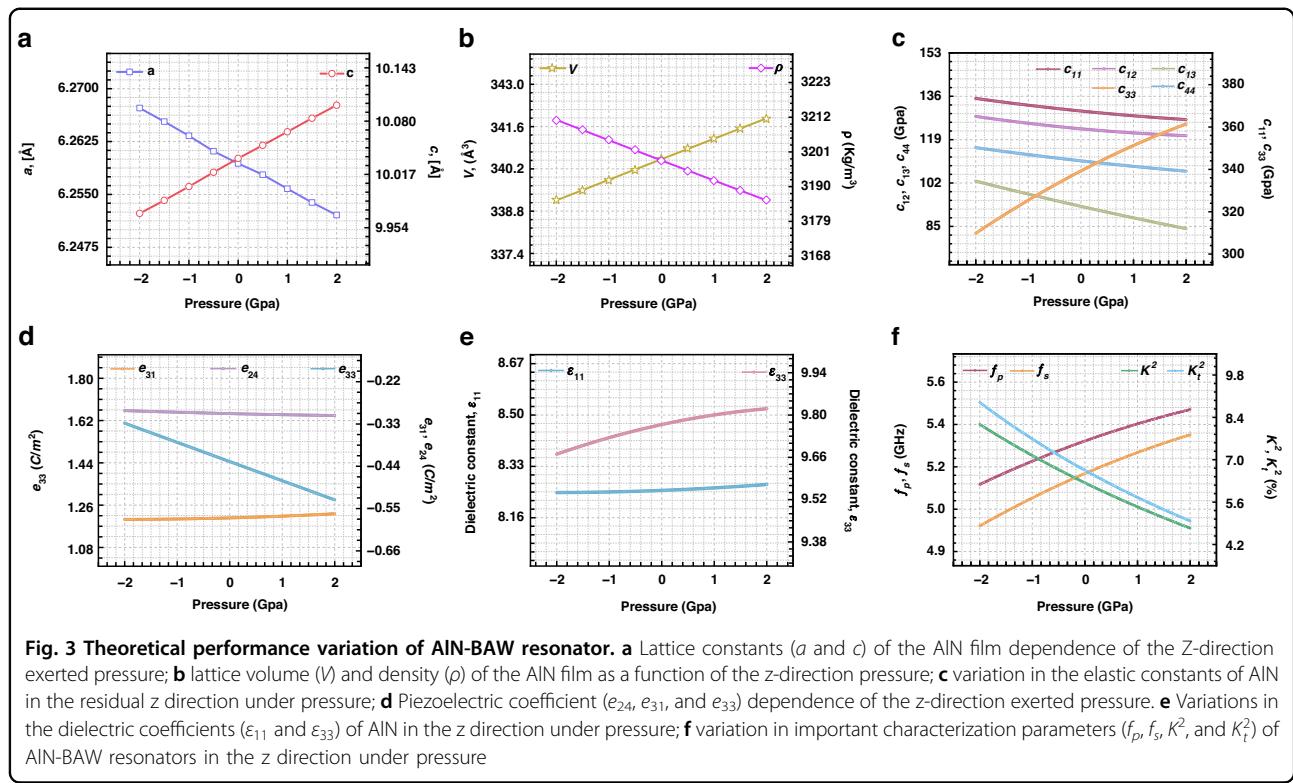
$$c_{44}(x) = 0.1391x^2 - 2.3071x + 110.687 \quad (6)$$

Table 1 Deformation of piezoelectric films under microchannels with various water velocities (25 °C)

Velocity	3 cm/s	4 cm/s	5 cm/s
Peak displacement values	1.9 μm	2.1 μm	2.2 μm

Table 2 Deformation of piezoelectric films under microchannels with various liquids flowing at 5 cm/s (25 °C)

Liquid	Water	Diethyl ether	Ethanol	Ethylene glycol
Viscosity	0.91×10^{-3} Pa·s	0.224×10^{-3} Pa·s	1.074×10^{-3} Pa·s	1.61×10^{-2} PaPa·s
Peak displacement values	2.2 μm	1.38 μm	2.33 μm	4.9 μm



For the piezoelectric film used in BAW resonators, another crucial characteristic is the piezoelectric constant. Piezoelectricity is intimately linked to material polarization. In the absence of external fields, the overall macroscopic polarization (P) in a piezoelectric material consists of two components: strain-induced or piezoelectric polarization (δP) and spontaneous polarization (P^s). The piezoelectric polarization is defined as²⁷

$$\delta P_i = \sum_j e_{ij} s_j \quad (7)$$

where e is the piezoelectric stress coefficient. Since precision BAW resonators mainly use e_{33} to create vibrations along the z-axis, in this work, we only examine polarizations along the (0001) axis. In the c-axis orientation of AlN, the piezoelectric polarization can be simply expressed as²⁸

$$\delta P_3 = e_{33} s_3 + e_{31} (s_1 + s_2) \quad (8)$$

where $s_1 = s_2 = (a - a_0)/a_0$ is the in-plane strain and $s_3 = (c - c_0)/c_0$ is the strain along the c-axis. c_0 and a_0 are the lattice constants in the equilibrium structure. Equation (8) is a macroscopic phenomenological equation. From a microscopic perspective, we separate the

clamped ion term and the internal relaxation term²⁹:

$$e_{33} = e_{33}^{(0)} + \frac{\delta P_3}{\delta u} \bigg|_{s_3} \frac{du}{ds_3}, \quad (9)$$

$$e_{31} = e_{31}^{(0)} + \frac{\delta P_3}{\delta u} \bigg|_{s_1} \frac{du}{ds_1}, \quad (10)$$

where

$$e_{33}^{(0)} = \frac{\delta P_3}{\delta s_3} \bigg|_u = c_0 \frac{\partial P_3}{\partial c}, \quad (11)$$

$$e_{31}^{(0)} = \frac{\delta P_3}{\delta s_1} \bigg|_u = \frac{a_0}{2} \frac{\partial P_3}{\partial a}, \quad (12)$$

The internal parameter u is defined as the bond length between anions and cations along the c-axis, and it determines the relative positions of atoms within the cell. Polarization changes caused linearly by relative sublattice shifts (variations in u) can be measured by the effective charge Z^* :

$$Z^* = \frac{\sqrt{3} a_0^2}{4e} \frac{\delta P_3}{\delta u} \bigg|_{s_3} \quad (13)$$

where e is the electronic charge. According to formulas (9)–(13), the piezoelectric coefficients and the lattice constants are closely related.

Using the Vienna Ab initio Simulation Package (VASP), a set of piezoelectric coefficients was calculated for AlN lattices deformed under various pressures. After the influence of pressure applied in the z-direction on the piezoelectric coefficient is analyzed, their relationship can be approximated via a quadratic equation, as illustrated in Fig. 3d. The corresponding equations are fitted as follows:

$$e_{33}(x) = 5.714 \times 10^{-5}x^2 - 0.0816x + 1.446 \quad (14)$$

$$e_{31}(x) = 8.857 \times 10^{-4}x^2 + 0.0037x - 0.574 \quad (15)$$

$$e_{15}(x) = e_{24}(x) = 3.57 \times 10^{-4}x^2 - 0.00318x - 0.303 \quad (16)$$

Additionally, the effect of pressure applied in the z-direction on the dielectric permittivity is investigated, as shown in Fig. 3e. Within the pressure range of -2 GPa to 2 GPa, the variation in relative permittivity with pressure (x) in the z-direction is described by quadratic Eqs. (17) and (18) in the following form:

$$\epsilon_{11}(x) = 1.57 \times 10^{-3}x^2 + 0.0067x + 8.25 \quad (17)$$

$$\epsilon_{33}(x) = -1.01 \times 10^{-2}x^2 + 0.045x + 9.77 \quad (18)$$

These physical parameter formulas directly reflect the effect of pressure applied in the z-direction on the performance of piezoelectric devices, such as BAW resonators and filters. For MEMS BAW resonators, the frequency and bandwidth are extremely tightly controlled. The frequency and bandwidth of BAW resonators are limited by the elastic constant (c_{33}), dielectric permittivity (ϵ_{33}), and piezoelectric coefficient (e_{33} ³⁰). The corresponding formula is as follows³¹:

$$Z = \frac{1}{jwC_0} \left(1 - K_t^2 \frac{kd/2}{\tan(kd/2)} \right) \quad (19)$$

where Z is the input impedance; w is the angular frequency; C_0 is the electrostatic capacitance; d is the film thickness of the device; K_t^2 is the piezoelectric coupling constant of the transversely clamped material ($K_t^2 = e^2/(c^E + \frac{e^2}{\epsilon^S})\epsilon^S = K^2/K^2 + 1$, where $K^2 = e^2/c^E\epsilon^S$ is the electromechanical coupling factor³²); and k is the wavenumber. According to the variations in c and e with pressure, the variations in K_t^2 and K^2 of AlN with pressure were calculated. They increase with increasing pressure, as shown in Fig. 3f. Since infinite input impedance corresponds to the parallel resonance of the lossless circuit, the corresponding acoustic frequency (f_p) is given

by

$$f_p = (2n + 1) \frac{v^D}{2d}, n = 0, 1, 2, \dots \quad (20)$$

where $v^D = \sqrt{c^E/\rho(K^2 + 1)}$ is the acoustic velocity in the piezoelectric medium. The series resonant frequency (f_s) is similarly obtained from Eq. (19) for $Z=0$ and is therefore obtained from

$$K_t^2 = \frac{\frac{\pi f_s}{2f_p}}{\tan\left(\frac{\pi f_s}{2f_p}\right)} \approx \frac{\pi^2 f_s}{4f_p} \frac{(f_p - f_s)}{f_p} \quad (21)$$

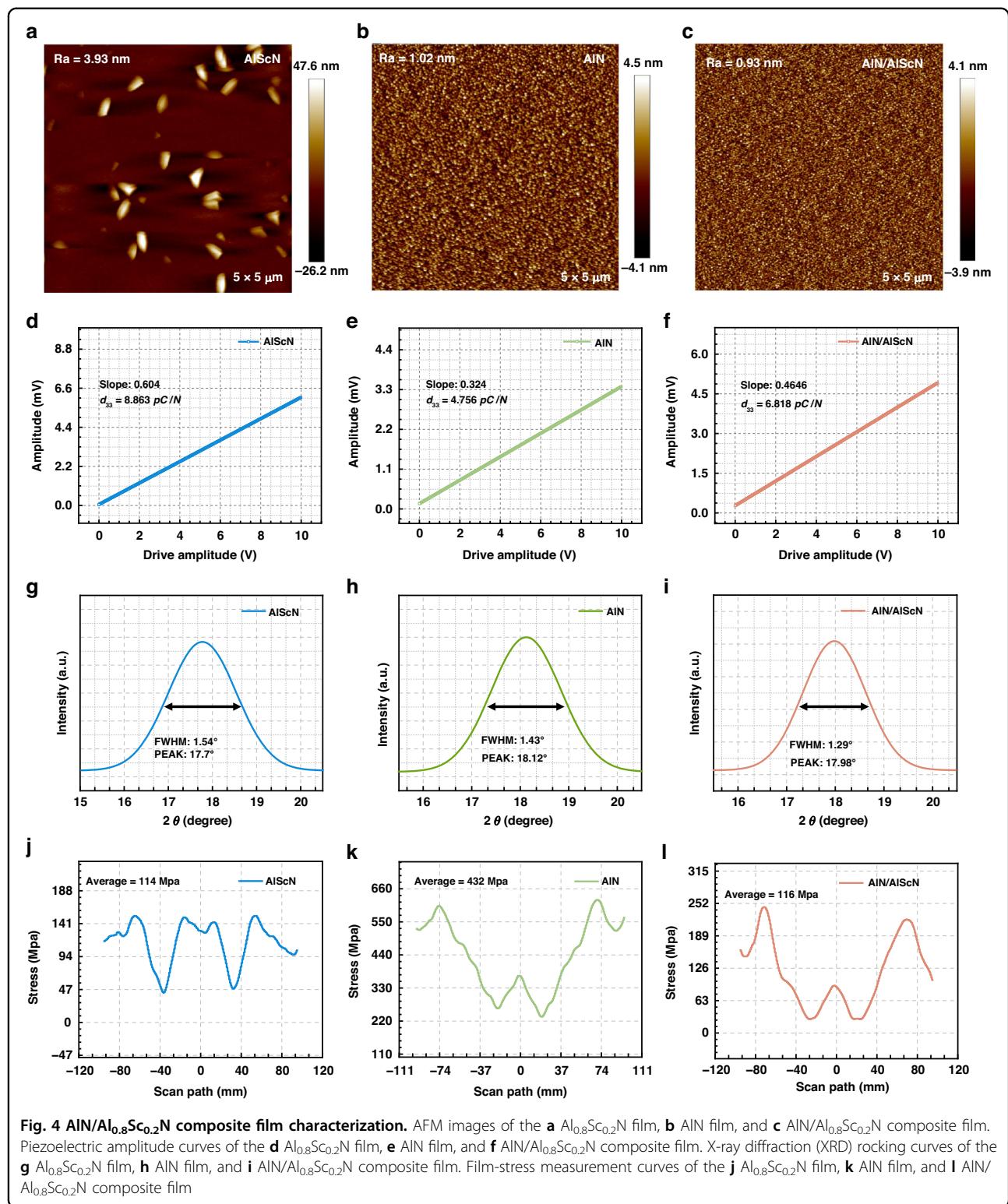
In this sensor, which is based on BAW resonators, the first resonator frequency is used; therefore, n is equal to 0. Based on the $1\text{ }\mu\text{m}$ thick AlN film and the above equations, the ideal variations in f_p and f_s with pressure applied in the z direction can be obtained, as shown in Fig. 3f. They increase with increasing pressure applied in the z-direction, and the increasing trend of f_s is greater than that of f_p , which is in agreement with the experimental study of Zhou et al.¹⁹.

Results and discussion

Film Fabrication and Characterization

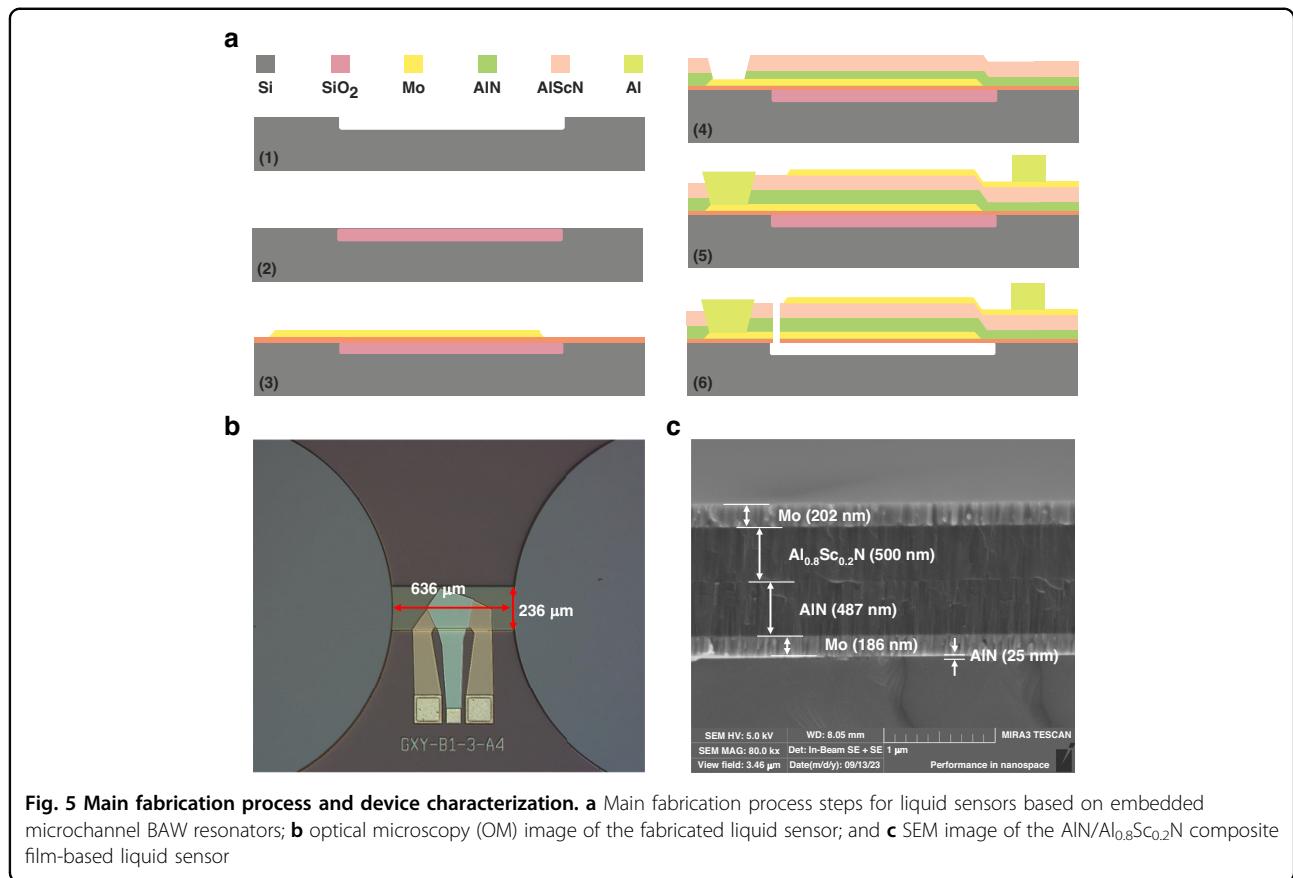
The piezoelectric properties of materials strongly influence the mechanical quality factors (Q_M), f_p , and K_t^2 of piezoelectric resonators³³. Wei Wu et al. reported that the $-\Delta f/f$ of piezoelectric plate sensors increased with increasing electromechanical coupling constant k_{31} due to the extrinsic effect of polarization orientation switching at room temperature³⁴. A. Talbi et al. also indicated that a better K_t^2 of the resonator could increase the sensitivity of the resonant sensor³⁵. AlScN, which enhances the piezoelectric property of AlN, has been used to fabricate resonant sensors that are more sensitive than those based on AlN³⁶. However, during the deposition of the AlScN film by the RF magnetron sputtering system, there are numerous abnormally oriented grains (AOGs). As demonstrated in Fig. 4a, atom force microscopy (AFM) revealed that the AOGs were large triangular pyramidal grains randomly distributed on the surface of the $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$ film. AOGs affect the piezoelectric and mechanical properties of AlScN films³⁷.

Therefore, this work utilized an AlN/ $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$ composite film (500 nm AlN + 500 nm $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$) to inhibit the growth of AOGs, which was investigated in our previous research³⁸. A $1\text{ }\mu\text{m}$ AlN, $1\text{ }\mu\text{m}$ $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$, and $1\text{ }\mu\text{m}$ AlN/ $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$ composite film (500 nm AlN + 500 nm $\text{Al}_{0.8}\text{Sc}_{0.2}\text{N}$) was prepared through an RF magnetron sputtering system. During deposition, the distance between the target and the substrate was 50 mm, and the deposition temperature was 200 °C. According to the



AFM characterization results, no AOGs exist on the AlN/Al_{0.8}Sc_{0.2}N composite film, and the AlN/Al_{0.8}Sc_{0.2}N composite film has a relatively small root-mean-square (rms) roughness (AlScN: 3.93 nm; AlN: 1.02 nm; AlN/Al_{0.8}Sc_{0.2}N:

0.93 nm), as depicted in Fig. 4a–c. This smooth film surface reduces scattering losses, thereby improving the Q value of the resonator³⁹. Through piezoresponse force microscopy (PFM), the piezoelectric



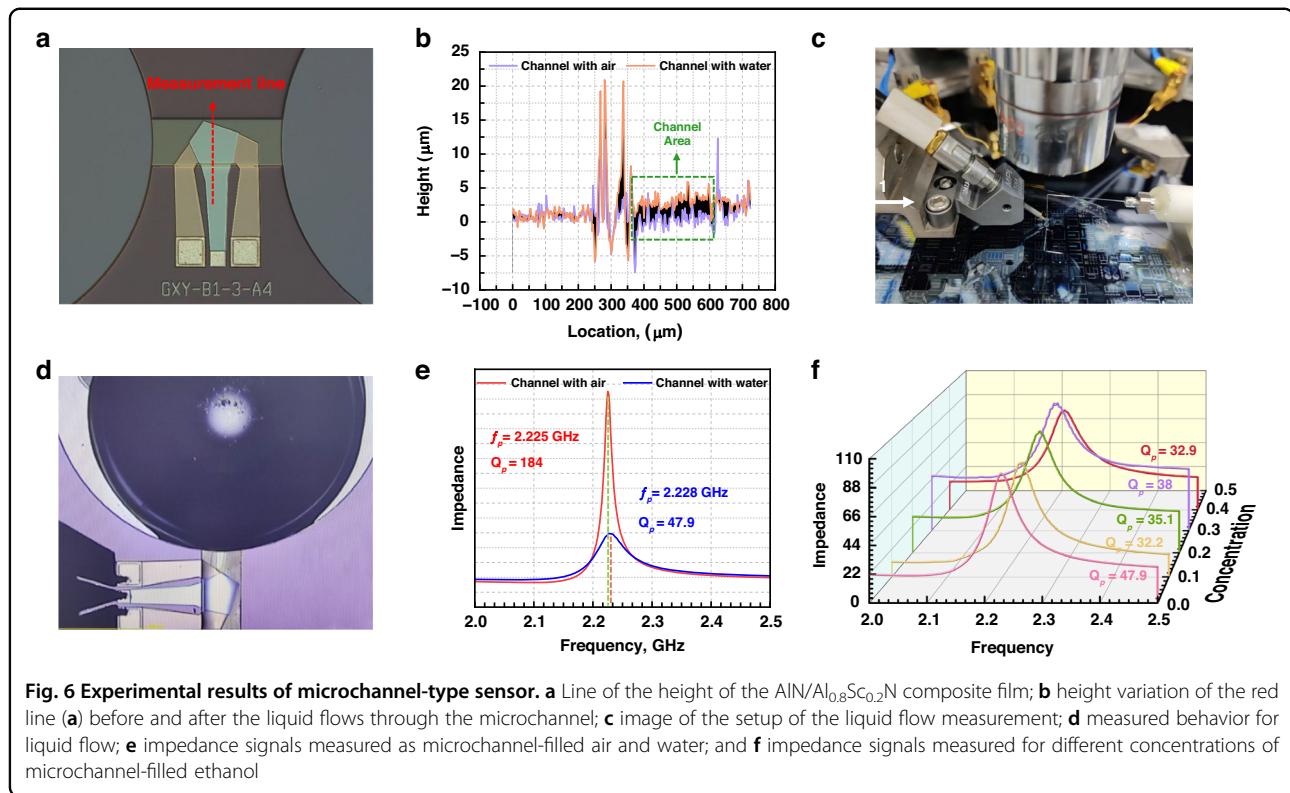
properties (d_{33}) of the AlN film, the Al_{0.8}Sc_{0.2}N film, and the AlN/Al_{0.8}Sc_{0.2}N composite film were measured, as shown in Fig. 4d-f. It is reasonable that $d_{33} = 6.818 \text{ pC/N}$ of the AlN/Al_{0.8}Sc_{0.2}N composite film is in the middle position among them. Moreover, the AlN/Al_{0.8}Sc_{0.2}N composite film improved the film quality of the piezoelectric layer in the BAW resonators. The full width at half maximum (FWHM) of the X-ray diffraction (XRD) rocking curves was used to characterize the film quality of these three piezoelectric films. As shown in Fig. 4g, h, and i), the FWHMs of the AlN film, Al_{0.8}Sc_{0.2}N film, and AlN/Al_{0.8}Sc_{0.2}N film were 1.43°, 1.54°, and 1.29°, respectively, which confirmed that the AlN/Al_{0.8}Sc_{0.2}N composite film had better crystal quality. In addition, the AlN/Al_{0.8}Sc_{0.2}N composite film neutralized the residual stress from the AlN film and the Al_{0.8}Sc_{0.2}N film, as demonstrated in Fig. 4j-l. An AlN/Al_{0.8}Sc_{0.2}N composite film could be an alternative for regulating the residual stress of a film to reduce the damage caused by residual stress in MEMS devices.

Fabrication and experiments

Based on this sensor design, the fabrication process is illustrated in Fig. 5a. The high-sensitivity liquid sensor decreased the fabrication cost because the same

fabrication process (6 masks) was used for the BAW resonators. (1) A 2.5 μm microchannel pool was etched by deep reactive ion etching (DRIE). (2) Then, the 3.5 μm released SiO₂ layer was deposited via plasma-enhanced chemical vapor deposition (PECVD), and the excess SiO₂ beside the swimming pool was removed through chemical mechanical polishing (CMP). (3) An RF magnetron sputtering system was used to deposit a 25 nm AlN seed film and a 200 nm Mo film. The Mo film is subsequently patterned and etched as bottom electrodes. (4) AlN and Al_{0.8}Sc_{0.2}N piezoelectric films were deposited successively. Inductively coupled plasma (ICP) was used to etch the AlN/Al_{0.8}Sc_{0.2}N composite film to expose the pads of the bottom electrodes. (5) The top Mo film was deposited and patterned as top electrodes. The Al film was evaporated and then peeled off into the pad shape. (6) The AlN/Al_{0.8}Sc_{0.2}N composite film was etched to form a release hole, and SiO₂ in the microchannel pool and liquid hole was released via VHF. The embedded microchannel sensor under the BAW resonators was fabricated as shown in Fig. 5b. A scanning electron microscope (SEM) image of the cross-sectional BAW resonator is shown in Fig. 5c.

Before testing, the height variation of the AlN/Al_{0.8}Sc_{0.2}N composite film along the red line was



measured via confocal laser scanning microscopy (CLSM), as shown in Fig. 6a, b. This film height variation could reflect the film deformation before and after the liquid flows through the microchannel. When liquid water flows through it, the film on the microchannel bulges due to upward pressure, as demonstrated in Fig. 6b. These measurement results are in agreement with the theoretical calculations and simulation results.

The liquid flow impacts on the BAW resonator were measured via the setup illustrated in Fig. 6c. This setup pushed a fixed amount of liquid through the spiral annotation tube to drop into the liquid hole. The droplet pressure drives the solution to flow through the microchannel, as shown in Fig. 6d. First, the BAW resonator was measured in air by a Keysight network analyzer (N5222B) with a Cascade Microtech GSG probe station (Cascade, USA). This impedance signal measured as microchannel-filled air is depicted in Fig. 6e. While the GSG probe remained tested, we pushed water into the liquid hole. Therefore, the impedance signal can eliminate the influence of other interference. As shown in Fig. 6e, f_p increased at 3 MHz, and Q_p decreased sharply from 184 to 47.9 as water flowed. This reduction in Q_p occurred because the liquid hindered the vibration of the BAW resonator and increased the energy loss of the BAW resonator. This frequency draft originating from the bulged AlN/

Al_{0.8}Sc_{0.2}N composite film confirms the accuracy of the first-principles calculation.

Subsequently, different concentrations of ethanol solutions were used to measure the sensitivity of this sensor. Figure 6f shows the impedance variations of the BAW resonator at different ethanol mass percentage concentrations (10%, 20%, 30%, and 40%). A noticeable frequency shift is observed with increasing ethanol concentration, and the quality factor (Q_p) fluctuates with increasing ethanol concentration. Figure 7a shows the variation in f_p as a function of the ethanol concentration. After linear approximation, the measured frequency variation under ethanol concentration was 0.51 MHz/%, and the corresponding concentration sensitivity ($\Delta f/f_p$) was 211 ppm/%, with an ultrahigh linearity of 0.995, as illustrated in Fig. 7b.

Conclusions

Based on the pressure of liquid flow on the microchannel wall, this work designed and fabricated a high-sensitivity resonant liquid sensor with an embedded microchannel under BAW resonators. Through FEM simulations, it was determined that at the same flow rate, different viscosities of liquids caused different pressures on the microchannel wall. As the viscosity of the liquid increased, the deformation of the membrane wall also increased. When the liquid flows in the microchannel, the

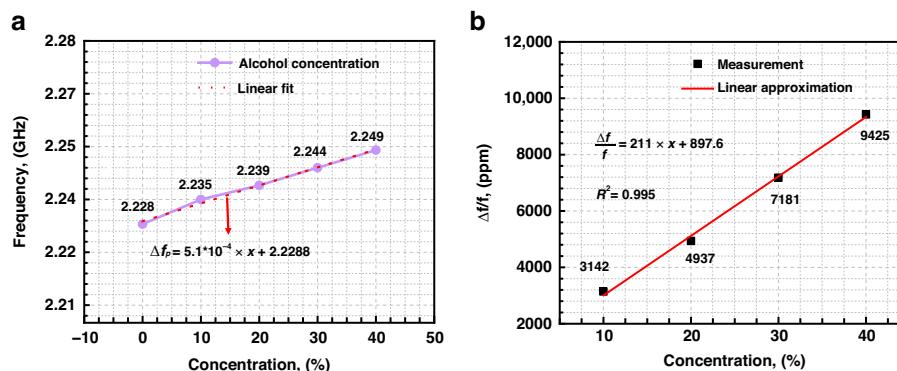


Fig. 7 Sensitivity of microchannel-type sensor. **a** Frequency variation under different concentrations of microchannel-filled ethanol and **b** sensitivity ($\Delta f/f_p$) of this microchannel liquid sensor

main force that causes the film to bulge is the z-direction pressure. Through first-principles calculations, we characterized the physical properties of the 32-atom hexagonal supercell of wurtzite AlN under different pressures in the z direction. These calculation results reveal the variation rule of the lattice constant, density, elastic constant, piezoelectric constant, etc. Subsequently, we revealed the intrinsic mechanism of how the z-direction pressure affects the performance of AlN-based BAW resonators. Theoretically, the upwardly convexness of the piezoelectric film caused by liquid flow can increase the resonator frequency.

During fabrication, the liquid sensor used an AlN/Al_{0.8}Sc_{0.2}N composite film to effectively suppress the abnormal orientation of the AlScN grains. The experimental results with different concentrations of ethanol reveal that our sensor, operating at a high resonant frequency of 2.225 GHz, achieves a remarkable sensitivity of 5.1 MHz/% (221 ppm/%) with an ultrahigh linearity of 0.995. These results of the frequency shift trend of the resonator are in agreement with the theoretical prediction. This study reveals the intrinsic mechanism of force sensing based on BAW resonators and offers insights for future research and development in this field.

Acknowledgements

This work was supported by the National Key Research and Development Program of China (Grant No. 2023YFF0723000), the National Natural Science Foundation of China (Grant No. 62201405) and the Key R&D Program of Hubei Province under Grant No. 2022BAA049 and the China Postdoctoral Science Foundation (Grant No. 2023T160496). The numerical calculations in this paper were performed on the supercomputing system at the Supercomputing Center of Wuhan University.

Author details

¹Key Laboratory of Artificial Micro, and Nano-structures of Ministry of Education, School of Physics and Technology, Wuhan University, Wuhan 430072, PR China. ²School of Mathematical and Physical Sciences, Wuhan Textile University, Wuhan 430200, PR China. ³The Institute of Technological Sciences, Wuhan University, Wuhan 430072, PR China. ⁴School of Microelectronics, Wuhan University, Wuhan 430072, PR China

Conflict of interest

The authors declare no competing interests.

Received: 29 May 2024 Revised: 24 July 2024 Accepted: 13 August 2024
Published online: 11 October 2024

References

- Connolly, D. & Paull, B. Rapid determination of nitrate and nitrite in drinking water samples using ion-interaction liquid chromatography. *Anal. Chim. Acta* **441**, 53–62 (2001).
- Nikolic-Jaric, M. et al. Microwave frequency sensor for detection of biological cells in microfluidic channels. *Biomicrofluidics* **3**, 34103 (2009).
- Liang, Y. et al. Wireless microfluidic sensor for metal ion detection in water. *ACS Omega* **6**, 9302–9309 (2021).
- Schwerthofer, U., Weigel, R. & Kissinger, D. in 2013 IEEE MTT-S International Microwave Workshop Series on RF and Wireless Technologies for Biomedical and Healthcare Applications. 1–3 (IEEE).
- Javed, A., Arif, A., Zubair, M., Mehmood, M. Q. & Riaz, K. A low-cost multiple complementary split-ring resonator-based microwave sensor for contactless dielectric characterization of liquids. *IEEE Sens. J.* **20**, 11326–11334 (2020).
- Mohammadi, S., Adhikari, K. K., Jain, M. C. & Zarifi, M. H. High-resolution, sensitivity-enhanced active resonator sensor using substrate-embedded channel for characterizing low-concentration liquid mixtures. *IEEE Trans. Microw. Theory Tech.* **70**, 576–586 (2021).
- Rey-Mermet, S., Lanz, R. & Muralt, P. Bulk acoustic wave resonator operating at 8 GHz for gravimetric sensing of organic films. *Sens. Actuators B* **114**, 681–686 (2006).
- Xuan, W. et al. Bulk acoustic wave resonator based wireless and passive pressure sensor. *Vacuum* **178**, 109433 (2020).
- Benes, E., Gröschl, M., Burger, W. & Schmid, M. Sensors based on piezoelectric resonators. *Sens. Actuators A* **48**, 1–21 (1995).
- Zhao, Z. et al. Design considerations for frequency shifts in a laterally finite FBAR sensor in contact with the newtonian liquid. *IEEE Trans. Ultrason. Ferroelectr. Freq. Control* **67**, 2402–2412 (2020).
- Ebrahimi, A., Withayachumnankul, W., Al-Sarawi, S. & Abbott, D. High-sensitivity metamaterial-inspired sensor for microfluidic dielectric characterization. *IEEE Sens. J.* **14**, 1345–1351 (2013).
- Yan, Z. et al. Material and device properties of ZnO-based film bulk acoustic resonator for mass sensing applications. *Appl. Surf. Sci.* **253**, 9372–9380 (2007).
- He, X. L. et al. Film bulk acoustic resonator pressure sensor with self temperature reference. *J. Micromech. Microeng.* **22**, 125005 (2012).
- Link, M. et al. Solidly mounted ZnO shear mode film bulk acoustic resonators for sensing applications in liquids. *IEEE Trans. Ultrason. Ferroelectr. Freq. Control* **53**, 492–496 (2006).

15. Vorobiev, A. & Gevorgian, S. Ferroelectric film bulk acoustic wave resonators for liquid viscosity sensing. *J. Appl. Phys.* **114**, 084106 (2013).
16. Rezazadeh, G. & Ghanbari, M. On the mathematical modeling of a MEMS-based sensor for simultaneous measurement of fluids viscosity and density. *Sens. Imaging* **19**, 1–20 (2018).
17. Chen, Y.-C., Chang, W.-T., Kao, K.-S., Yang, C.-H. & Cheng, C.-C. The liquid sensor using thin film bulk acoustic resonator with c-axis tilted AlN films. *J. Nanomater.* **2013**, 2–2 (2013).
18. Liang, J. et al. On-chip nanofluidic integration of acoustic sensors towards high Q in liquid. *Appl. Phys. Lett.* **111**, 203501 (2017).
19. Zhou, Y. et al. Investigation of film bulk acoustic resonators for sensing applications in liquid environment. *Appl. Phys. Lett.* **121**, 213501 (2022).
20. Yu, H., Pang, W., Zhang, H. & Kim, E. S. in *IEEE International Conference on Micro Electro Mechanical Systems*. 28–31 (IEEE).
21. Wang, J., Zheng, Y. & Ansari, A. Ferroelectric aluminum scandium nitride thin film bulk acoustic resonators with polarization-dependent operating states. *Phys. Status Solidi (RRL)* **15**, 2100034 (2021).
22. Segall, M. D. et al. First-principles simulation: ideas, illustrations and the CASTEP code. *J. Phys.* **14**, 2717 (2002).
23. Clark, S. J. et al. First principles methods using CASTEP. *Z. Kristallogr. Crystall. Mater.* **220**, 567–570 (2005).
24. Wickramaratne, D., Bernstein, N. & Mazin, I. I. Impact of biaxial and uniaxial strain on V₂O₃. *Phys. Rev. B* **100**, 205204 (2019).
25. Pfrommer, B. G., Côté, M., Louie, S. G. & Cohen, M. L. Relaxation of crystals with the quasi-Newton method. *J. Comput. Phys.* **131**, 233–240 (1997).
26. Sharma, H., Kreisel, J. & Ghosez, P. First-principles study of PbTiO₃ under uniaxial strains and stresses. *Phys. Rev. B* **90**, 214102 (2014).
27. Nye, J. F. *Physical Properties of Crystals: Their Representation by Tensors and Matrices*. (Oxford university press, 1985).
28. Posternak, M., Baldereschi, A., Catellani, A. & Resta, R. Ab initio study of the spontaneous polarization of pyroelectric BeO. *Phys. Rev. Lett.* **64**, 1777 (1990).
29. Dal Corso, A., Posternak, M., Resta, R. & Baldereschi, A. Ab initio study of piezoelectricity and spontaneous polarization in ZnO. *Phys. Rev. B* **50**, 10715 (1994).
30. Liu, Y. et al. Materials, design, and characteristics of bulk acoustic wave resonator: a review. *Micromachines* **11**, 630 (2020).
31. Rosenbaum, J. F. *Bulk Acoustic Wave Theory and Devices*. (Artech House Acoustics Library, 1988).
32. Hashimoto, K.-Y. *RF Bulk Acoustic Wave Filters for Communications*. (Artech House, 2009).
33. Zhang, S. & Yu, F. Piezoelectric materials for high temperature sensors. *J. Am. Ceram. Soc.* **94**, 3153–3170 (2011).
34. Wu, W., Shih, W. Y. & Shih, W.-H. Enhancing detection sensitivity of piezoelectric plate sensor by increasing transverse electromechanical coupling constant. *J. Appl. Phys.* **114**, 064505 (2013).
35. Talbi, A. et al. ZnO/quartz structure potentiality for surface acoustic wave pressure sensor. *Sens. Actuators A* **128**, 78–83 (2006).
36. Wang, H., Zhang, L., Zhou, Z. & Lou, L. Temperature performance study of SAW sensors based on AlN and AlScN. *Micromachines* **14**, 1065 (2023).
37. Liu, C. et al. Evaluation of the impact of abnormal grains on the performance of ScO₁₅AlO₈₅N-based BAW resonators and filters. *J. Micromech. Microeng.* **32**, 034002 (2022).
38. Gu, X. et al. Experimental and theoretical studies of effective piezoelectric coefficients of 2-2 connectivity AlN/AlScN composite piezoelectric films. *Compos. Commun.* **38**, 101502 (2023).
39. Bousquet, M. et al. in *IEEE International Ultrasonics Symposium*. 1–4 (IEEE).